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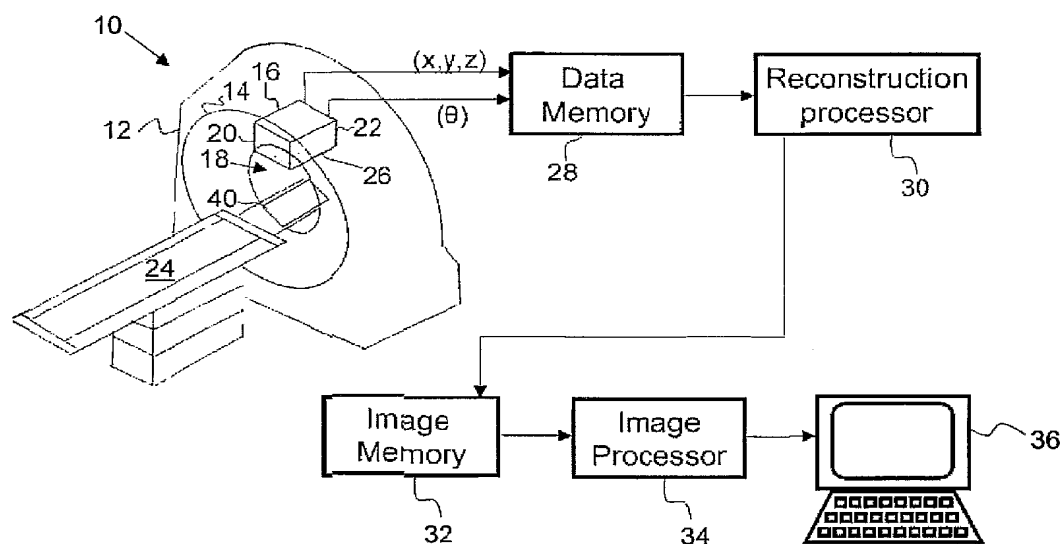
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[Continued on next page]

(54) Title: CALIBRATION METHOD AND APPARATUS FOR PIXILATED SOLID STATE DETECTOR



(57) Abstract: A system calibrates a solid state detector (20) for a radiation imaging device (10) in a single acquisition. A calibration phantom (40) emits radiation concurrently at at least first and second characteristic energy levels. A nuclear camera (16) generates associated sets of radiation data spanning both the first and second energy levels from the emitted radiation that is received by solid state detector (20). A means (64) determines associated centers of energy peaks and energy values of the generated data sets. A calibration means (80) calibrates at least one of gain, offset, performance and dead pixel correction based on the determined centers and peaks of the acquired data sets.

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## CALIBRATION METHOD AND APPARATUS FOR PIXILATED SOLID STATE DETECTOR

### DESCRIPTION

The present invention relates to the diagnostic imaging systems and methods. It finds particular application in conjunction with the nuclear imaging systems using solid state detectors (SSD) and will be described with particular reference thereto. It will be appreciated that the invention is also applicable to the other imaging systems using  
5 other pixilated imaging devices, and the like.

Diagnostic nuclear imaging is used to study a radionuclide distribution in a subject. Common use radiopharmaceuticals incorporate a variety of short lives radioisotopes. Each isotope has a characteristic energy, usually in the range of about 50-500 keV. Typically, one or more radiopharmaceuticals or radioisotopes, appropriate to the  
10 imaging examination, are selected and injected into the subject's bloodstream. Typical applications include imaging the circulatory system or imaging specific organs, which absorb the injected radiopharmaceutical. A radiation detector is placed adjacent to the surface of the subject to monitor and record emitted radiation. Often, the detector is rotated or indexed around the subject to monitor the emitted radiation from a plurality of  
15 directions. These projection data sets are reconstructed into a three-dimensional image representative of the radiopharmaceutical distribution within the subject.

Historically, each detector head included an array of photomultiplier tubes (PMTs) facing a large scintillation crystal. Each radiation event generated a corresponding flash of light that was being seen by the closest photomultiplier tubes. Each  
20 photomultiplier tube that saw an event put out a corresponding analog pulse. The analog pulses from the individual PMT's were digitized and combined to generate x and y spatial coordinates of the location of scintillation event on the crystal face.

In recent years, solid state detectors have been introduced in nuclear cameras. Solid state detectors utilize the photoelectric effect to detect radiation. More  
25 specifically, the received radiation photons liberate electrons from their orbits around atoms of the target material. The electrons are detected as an electrical signal.

Solid state detector based nuclear camera calibration is typically performed for gain and offset of each pixel to correct inconsistencies with pixel charge collection,

signal bias and impurities that interfere with charge generation in the pixels of the solid state detector. In addition, calibration might be required in regards to the dead pixel recovery and uniformity of amount of counts acquired within the acquisition window. For linearity over the radioisotope energy range, two calibrations are performed. A uniform sheet of a first isotope material, such as cobalt with an energy peak at 122keV, is placed in front of the detector and the radiation is detected for about an hour. Because the radiation source is uniform, all detectors should have the same response. Then, the first sheet is removed and the process is repeated for another hour with a uniform layer of a second isotope with a different characteristic energy, e.g. Americium with a 60keV peak. Based on the response of each detector at two offset energies, a calibration adjustment which is interpolated and extrapolated to be linear over the full range of common isotope energies is determined. In multi-head nuclear cameras, this process is repeated for each head. Although effective, the calibration process is time consuming.

There is a need for a technique that will perform the calibration more quickly and efficiently. The present invention provides a new imaging apparatus and method which overcomes the above-referenced problems and others.

In accordance with one aspect of the present invention, a system for calibrating a solid state detector for a radiation imaging device in a single acquisition is disclosed. A means emits radiation concurrently at at least first and second preselected energy levels. A means generates associated sets of radiation data spanning both the first and second energy levels from the emitted radiation that is received by solid state detector. A means determines associated centers of energy peaks and energy values. A means calibrates at least one of gain, offset, performance and dead pixel correction based on the determined centers and peak of the acquired data sets.

In accordance with another aspect of the present invention, a method of calibrating a solid state detector in a nuclear imaging system is disclosed. Radiation is emitted concurrently at at least first and second preselected energy levels. Associated sets of radiation data from the emitted radiation received by the detector are generated. Centers of energy peaks and energy values for the generated data sets are determined. At least one

of gain, offset, performance and dead pixel correction based on the determined centers and peaks of the acquired data sets is calibrated.

One advantage of the present invention resides in expediting calibration by shortening the calibration times.

5 Another advantage of the present invention resides in performing calibration for pixel gain and offset, uniformity, and dead pixel correction in a single acquisition thus providing more consistent calibration method.

Another advantage of the present invention resides in performing calibration for pixel gain and offset, uniformity, and dead pixel correction using only one  
10 isotope.

Still further advantages and benefits of the present invention will become apparent to those of ordinary skill in the art upon reading and understanding the following detailed description of the preferred embodiments.

15

The invention may take form in various components and arrangements of components, and in various steps and arrangements of steps. The drawings are only for purposes of illustrating the preferred embodiments and are not to be construed as limiting the invention.

20 FIGURE 1 is a diagrammatic illustration of a nuclear imaging system;  
FIGURES 2A is a detailed diagrammatic illustration of a first calibration phantom adjacent detector head;

FIGURE 2B is a detailed diagrammatic illustration of a second calibration phantom; and

25 FIGURE 3 is a diagrammatic illustration of a calibration system in accordance with the present invention.

30 With reference to FIGURE 1, a nuclear imaging device 10 typically includes a stationary gantry 12 that supports a rotating gantry 14. One or more detector heads 16 are carried by the rotating gantry 14 to detect radiation events emanating from a region of interest or examination region 18. Each detector head 16 includes a two-

dimensional array **20** of detector elements. The detector arrays are preferably solid-state detectors, which convert gamma radiation directly into electrical charge. Each head **16** includes circuitry **22** for converting each radiation response into a digital signal indicative of its location (x, y) on the detector face and its energy (z).

5                   Typically, an object to be imaged is injected with one or more radiopharmaceuticals or radioisotopes and placed in the examination region **18** supported by a couch **24**. The presence of the pharmaceuticals within the object produces emission radiation from the object. Radiation traveling along a trajectory defined by a collimator **26** is detected by each detector head **16**. The detector heads **16** are angularly indexed or  
10                   rotated around the examination region **18** to collect the emission data from a plurality of directions. During diagnostic imaging, the projection emission data (x, y, z) and an angular position ( $\theta$ ) of the detector head around the examination region are stored in a data storage **28**. A reconstruction processor **30** processes the event and detector orientation data from the data storage **28** into a volumetric image representation. The image representation  
15                   is then stored at a volume image memory **32** for manipulation by a video processor **34** and display on an image display **36** such as a video monitor, printer, or the like.

                  With continuing reference to FIGURE 1 and further reference to FIGURE 2A, a calibration phantom **40** is positioned and supported on the couch **24** in front of the detector head **16** to be imaged by the nuclear imaging device **10**. Typically, the phantom  
20                   has a horizontal size that corresponds to the size of the radiation receiving face of the detector head. The detector head to be calibrated is positioned at 12 o'clock to face the phantom **40** square on. The couch **24** is raised and, if possible, the detector head is lowered to bring the detector head and the phantom into close proximity. To obtain an accurate calibration, the phantom **40** emits radiation at at least two energy levels concurrently. The  
25                   phantom **40** includes a tank **42** positioned in front of the collimator **26**. The tank **42** includes a front side **44**, which is positioned facing the collimator **26** of the detector head, and a back side **46**, opposing the front side **44** and lying on the couch **24**. The tank **42** includes a first radiation source **48**, which is, preferably, a liquid solution Technetium (Tc) that is dispersed into the tank **42**. Technetium provides a first energy level, with a first peak  
30                   centered at about 140keV. Technetium is a common radiopharmaceutical isotope and calibrating to it specifically improves the correlation. However, other isotopes might be

used as well. Examples of such isotopes are Gallium (Ga) and Germanium (Ge) with corresponding energy peaks at about 500keV and 660keV.

A second source of radiation **50** with a different emission peak, such as removable lead (Pb) sheet or back sheet or back layer **52**, is positioned about the back side **46** of the tank **42**. The back sheet **52** might be inserted into a slot **54** provided in the tank **42**. The lead provides radiation with a second energy peak centered at about 70keV. More particularly, the second radiation is generated as backscattered emission radiation. When radiation from the first radiation source **48** collides with the solid lead sheet **52**, it causes secondary emission. Of course, other materials, such as tin and copper, are also contemplated to provide a source of secondary radiation.

In one alternate embodiment, the first radiation source **48** includes an isotope, such as Cobalt (Co), having two energy levels with the first energy peak at about 130keV and the second energy peak at about 122keV. In addition to the first and second energy peaks provided by Cobalt, a lead or other sheet at the back of the phantom **40** can provide a radiation source **50** with a third energy peak for more accurate calibration.

In general, calibration accuracy is improved by having more points along the calibration curve, particularly points which span the operating energy region.

In another embodiment, the first radiation source **48** is a liquid mixture or stacked of isotopes, concurrently emitting radiation at two or more energy levels. Optionally, the second radiation source **50** is a sheet that is attached to the phantom **40** to provide another energy level by secondary emission.

With reference to FIGURE 2B, an additional radiation source or front sheet or front layer **56** is attached to the front side **44** of the first radiation source **48**. The front sheet **56** is positioned directly in front of the collimator **26** for providing an increased secondary radiation flux. Preferably, the front layer is very thin, such as an electroplated or foil layer which is adhered to the front face of the tank **42**. The front layer **56** can be the same metal as the back layer **52** to provide more radiation at the second energy peak. Alternatively, a different metal which produces secondary radiation at yet another energy peak can be used.

With reference again to FIGURE 1 and further reference to FIGURE 3, the phantom **40** emits radiation at two or more energy levels or peaks. The data, indicative of radiation intensity produced by a first radiation source and a second radiation source for

each pixel or detector element with coordinates  $(x_i, y_j)$ , is collected into the data memory 28. The data is thresholded or sorted by a sorting means 60 to distinguish between the data contributed by the first and second energy peaks. The sorted data is stored in a sorted data memory 62. An energy peak means 64 finds the first and second energy peaks which correspond to the first and second radiation sources that have known energy levels. Specifically, a spectrum processor 66 processes each detector element's output to determine the energy of each photon and find the distribution of the radiation intensity. The distribution can be expressed as a curve of number of received photons counts vise energy. Such curve looks as a flat line with two Gaussian peaks – each centered on the energy peak for each radiation source, as shown in FIGURE 4. A best curve fitting means 68 uses a best curve fitting technique to determine the first and second measured energy peaks. Preferably, the best curve fitting means 68 uses Gaussian curve fitting function:

$$f(x) = C e^{-\frac{x-x_0}{2\sigma^2}},$$

where the parameters to be found are peak center  $x_0$ , height of an energy peak  $C$  and width of the energy peak  $\sigma$ .

A peak center determining means 70 finds the center positions  $C_1$  and  $C_2$  of the first and second measured energy peaks. An energy determining means 72 finds the values of energy  $E_1$  and  $E_2$  at the center positions of both peaks. The peak center positions and the energy values are stored in an energy peaks memory 74. A reference point determining means 76 calculates a gain and offset reference points such that the output curve of each detector element is aligned to a common reference, i.e. all the same center energy and peak amplitude. Optionally, gain and offset reference points are values entered by an operator.

A calibration means 80 retrieves the information from the reference point determining means 76 and the energy peaks memory 74 to determine calibration parameters for each element of the detector array 20. More particularly, a gain calibration means 82 calculates gain as

$$g = \frac{E_2 - E_1}{C_2 - C_1},$$

where  $C_1$  and  $C_2$  are centers of the curves and  $E_1$  and  $E_2$  are corresponding peak energy values.



An offset calibration means **84** calculates offset as

$$C_0 = C_1 - \frac{E_1}{g},$$

where  $C_1$  is the center of the curves and  $E_1$  is the corresponding energy value.

A performance means **86** looks at the each detector element data and  
5 compares it with predetermined performance measures to determine how efficient the  
detector is and how good the pixels energy resolution is. For example, it determines if any  
measured peak is too low or too wide relative to other detector elements. The performance  
means **86** uses a totality of performance parameters to perform additional calibration such  
as the correction of uniformity of the response of the detector.

10 A dead pixel recovery processor **88** monitors the information about each  
pixel to determine if each has substantially the same number of counts and substantially the  
same energy distribution. If any of the detector elements differ from others by more than a  
preselected deviation, the dead pixel recovery processor disconnects the malfunctioning  
elements from the circuitry **22**. The dead pixel recovery processor **88** creates a look up  
15 table, in which the outputs of neighboring detector elements are interpolated to fill in the  
dead pixel area.

The invention has been described with reference to the preferred  
embodiments. Modifications and alterations may occur to others upon a reading and  
understanding of the preceding detailed description. It is intended that the invention be  
20 constructed as including all such modifications and alterations insofar as they come within  
the scope of the appended claims or the equivalents thereof.

### CLAIMS

Having thus described the preferred embodiments, the invention is now claimed to be:

1. A system for calibrating a solid state detector (20) for a radiation imaging device (10) in a single acquisition, the system comprising:

a means (40) for emitting radiation concurrently at least first and second preselected energy levels;

a means (16) for generating associated sets of radiation data spanning both the first and second energy levels from the emitted radiation that is received by solid state detector (20);

a means (64) for determining associated centers of energy peaks and energy values of the generated data sets; and

a means (80) for calibrating at least one of gain, offset, performance and dead pixel correction based on the determined centers and peaks of the acquired data sets.

2. The system as set forth in claim 1, wherein the radiation emitting means (40) includes:

a tank (42), which holds a radioisotope which emits radiation at the first energy level; and

a means (50) which receives radiation of the first energy level and emits radiation at the second energy level.

3. The system as set forth in claim 2, wherein the radioisotope in is a liquid solution.

4. The system as set forth in claim 3, wherein the means (50), which emits radiation at the second energy level, includes:

a dense metal sheet (52) disposed along a rear side (46) of the tank (42) opposite the solid state detector (20), the dense metal sheet (52) emitting the second energy level radiation by secondary emission.

5. The system as set forth in claim 4, further including a second metal sheet (56) disposed along a front side (44) of the tank (42) between the radioisotope and the solid state detector (20), the second metal sheet (56) receiving radiation of the first energy level and emitting radiation of another energy level.

6. The system as set forth in claim 5, wherein the dense and second metal sheets (52, 56) include lead and emit secondary radiation at 70keV.

7. The system as set forth in claim 1, wherein the radiation emitting means (40) includes a single dual peak isotope which emits radiation at both the first and the second energy levels concurrently.

8. The system as set forth in claim 7, further including:  
a source of a secondary radiation (50), which converts some of the radiation emitted by the dual peak isotope to a characteristic energy level.

9. The system as set forth in claim 1, wherein the radiation emitting means (40) includes a mixture of isotopes, each isotope emitting radiation at at least one energy level.

10. The system as set forth in claim 9, further including:  
a source of a secondary radiation (50) which receives radiation from the isotope mixture and emits radiation at a characteristic energy level lower than the energy levels of at least some of the radiation emitted by the isotope mixture.

11. The system as set forth in claim 1, wherein the solid state detector (20) includes an array of detector elements and the generating means (16) generates a set of radiation data for each detector element.

12. A method of calibrating a solid state detector (20) in a nuclear imaging system (10) comprising:

concurrently emitting radiation at at least first and second preselected energy levels;

generating associated sets of radiation data from the emitted radiation received by the detector (20);

determining centers of energy peaks and energy values for the generated data sets; and

calibrating at least one of gain, offset, performance and dead pixel correction based on the determined centers and peaks of the acquired data sets.

13. A calibration phantom for a pixilated solid state detector, the phantom comprising:

a radioisotope layer which emits radiation of a first characteristic energy; and

a metal layer disposed parallel to the radioisotope layer to receive the radiation of the first characteristic energy from the radioisotope layer and emit radiation of a second characteristic energy by a secondary emission.

14. The calibration phantom as set forth in claim 13, wherein the radioisotope layer includes a radioisotope in liquid solution.

15. The calibration phantom as set forth in claim 14, wherein the liquid solution includes a plurality of radioisotopes each having a characteristic energy.

16. The calibration phantom as set forth in claim 14, wherein the radioisotope includes a radioactive isotope of at least one of Technetium, Gallium, Americium, Cobalt, and Germanium.

17. The calibration phantom as set forth in claim 13, wherein the metal layer is one of Lead, Copper, Molybdenum, Tungsten, and Tin.

18. The calibration phantom as set forth in claim 13, wherein the radioisotope has a dual energy peak.

19. In combination, the phantom of claim 13 and a pixilated nuclear camera, and further including:

a pixel energy peak analyzer which finds energy peaks generated about the first and second characteristic energies for each pixel of the pixilated nuclear camera; and

a calibration processor which utilizes the energy peaks information to at least one of correct each pixel's gain and offset, regulate the nuclear camera's overall performance, and recover dead pixels areas.

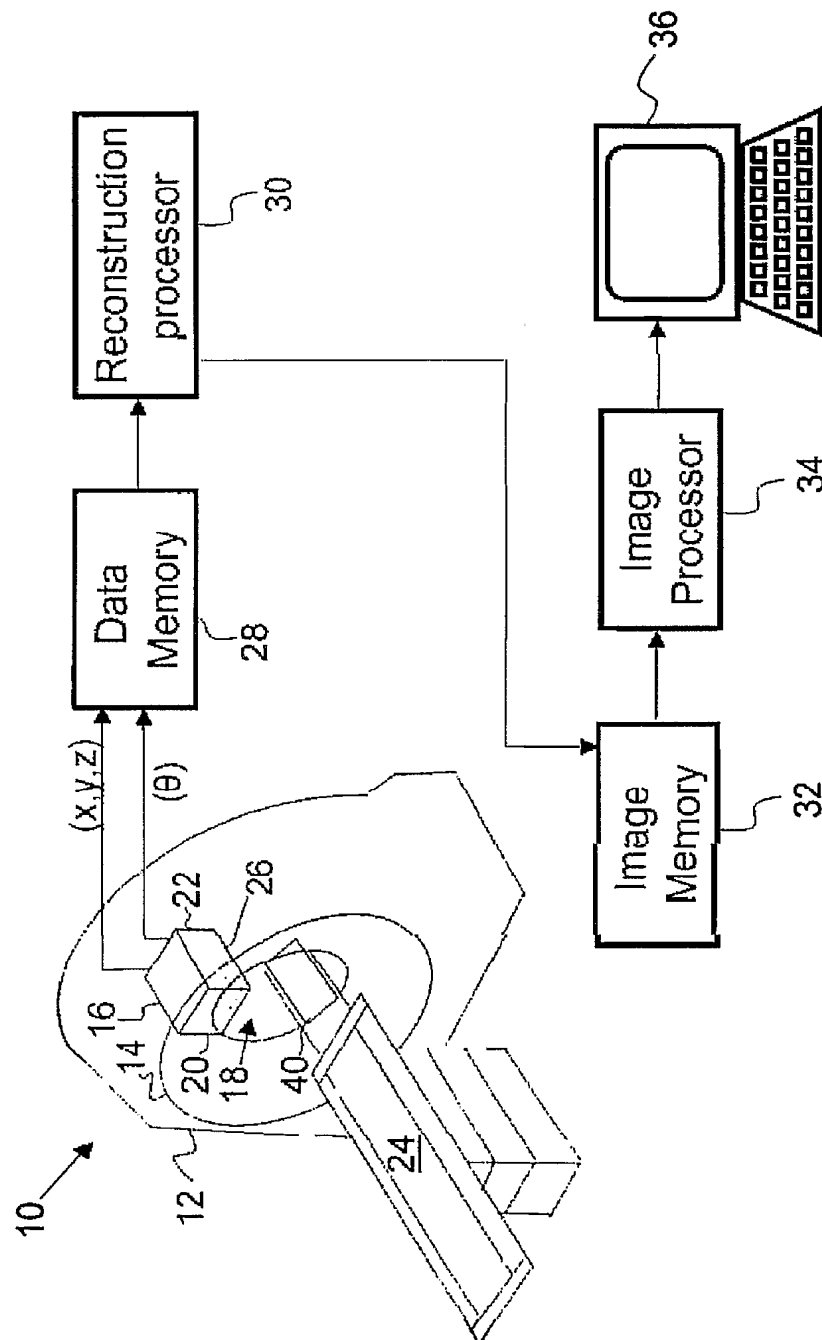


FIG 1

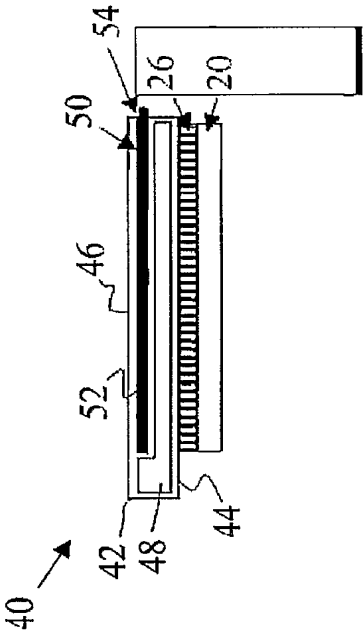


FIG 2A

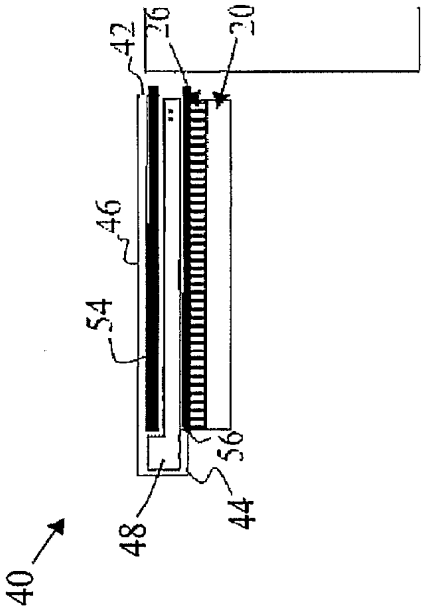


FIG 2B

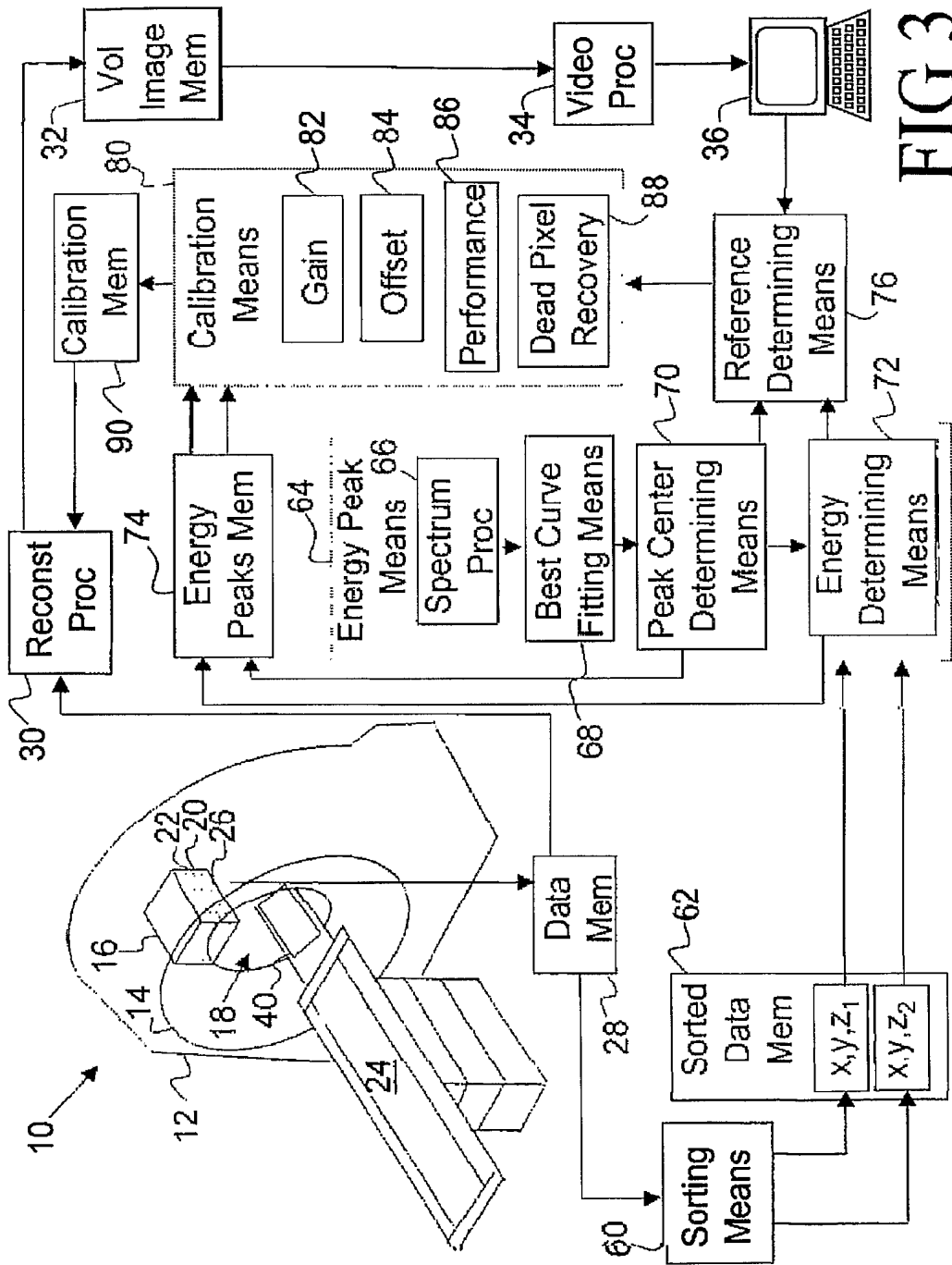


FIG 3



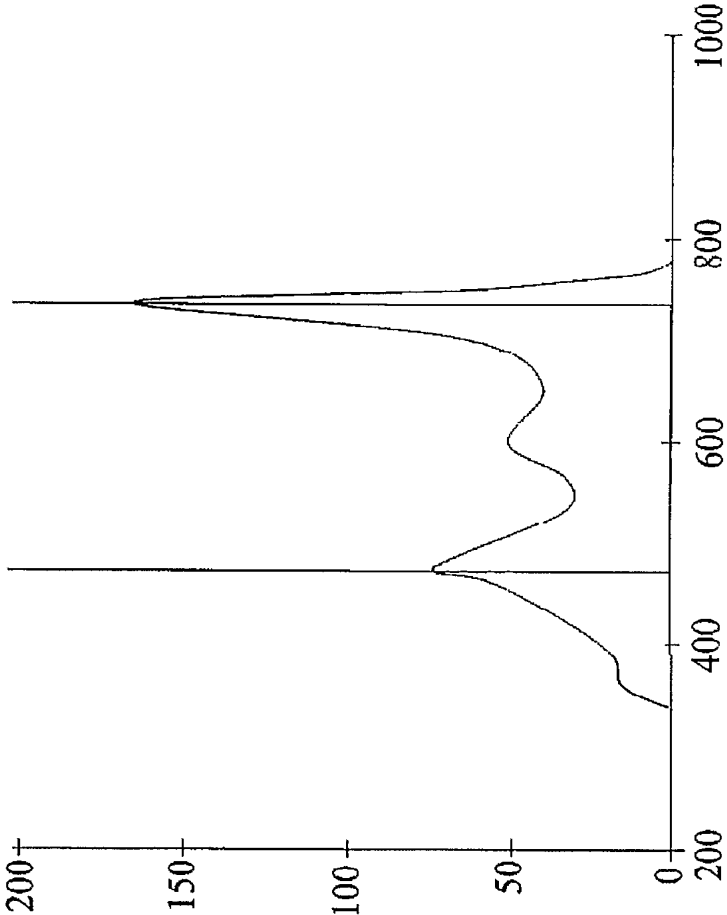



FIG 4

# INTERNATIONAL SEARCH REPORT

International Application No

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**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 7 G01T1/24

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 H01J G01T

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ, INSPEC, COMPENDEX, BIOSIS

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
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Y		2-6,8-10,14,15,19
Y	GB 1 382 780 A (I FIZ AKADEMII NAUK GRUZINSKOI) 5 February 1975 (1975-02-05)  page 1, line 92 - page 2, line 89 page 3, line 5 - line 29 page 3, line 70 - page 4, line 43  ----- -/--	2-6,8-10,14,15,19

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

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- \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
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Date of the actual completion of the international search

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Name and mailing address of the ISA

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# INTERNATIONAL SEARCH REPORT

International Application No  
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## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
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Information on patent family members

International Application No

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